# **Introduction**

Abnormal iron regulation in neural tissues is implicated in numerous neurodegenerative conditions [1]. Visualization and quantification of brain iron could enable clinical exploitation of this biomarker.

The transverse relaxation rate  $(R_2)$  is correlated with iron concentration and increases linearly with field strength as a result of iron  $[2, 3]$ . Direct  $R_2$  measurements are confounded by water content while high field specific acquisition and processing challenges preclude widespread implementation.

We revisit the variable interecho spacing (ESP) method for iron detection [4, 5] at | high field using recent methodological advances. We investigate the relationships between relaxation rates, their interecho dependence, and non-heme brain iron at 4.7 T to elucidate the merits of transverse relaxometry with single or multiple ESP for iron detection.

We employed the  $B_1$  insensitive multiecho spin echo  $R_2$  mapping method [6] to image a single slice  $(1.5 \times 1.5 \times 4.5 \text{ mm}^3)$  through the basal ganglia of seven healthy volunteers (40±9.6 years old; 6 m, 1 f) at 4.7 T.

R<sub>2</sub> maps were obtained with ESPs of 6.0, 10, 15, 20, 30, and 45 ms; echo trains were 180 ms long, except ESP=6 ms, which was 120 ms. TR was 2.8 s; all other parameters were held constant.

Region-of-interest (ROI) analysis was performed on frontal white matter (WM), frontal gray matter (GM), occipital GM, caudate nucleus, putamen, globus pallidus, and thalamus to obtain average R<sub>2</sub> values. Two analyses were performed:



# **Results (continued)**

With variable ESP, a linear increase in slope is observed with non-heme iron, Fig 3b. A lower correlation coefficient ( $R^2$ =0.42) is measured than with  $R_2$  vs. iron, but systematic regional bias is reduced and an insignificant baseline is observed.

i)  $R_2$  values measured with ESP=6 ms were correlated with non-heme iron levels, estimated from a post-mortem study accounting for brain region and subject age [7]. ii) Regression of R<sub>2</sub> versus log(ESP) was performed to obtain a slope; these slopes were then correlated to estimated non-heme iron levels.

### **Methods**

 $T_2$ -weighted images and  $R_2$  maps obtained with ESP=6 and 30 ms are shown in Fig 1. Hypo-intensity in the globus pallidus (red arrow) is visible at ESP=6 ms and obvious at 30 ms; quantitative ROI analysis reveals a near linear increase in  $R_2$  as a function of  $log(ESP)$  in all regions measured, Fig 2. Regression of  $R_2$  vs. non-heme iron provides a high correlation coefficient ( $R^2=0.77$ ), but yields a non-zero intercept and three regions (FWM, OGM, Thalamus) are offset from a stronger linear trend through the remaining regions, Fig 3a.

Figure 2: R<sub>2</sub> versus ESP for seven Figure 3: Fig. 3: (a) R2 with ESP=6 ms **brain regions, as labeled, for a healthy (first points on Fig. 2) and (b) Slope of R2 vs. ESP against brain iron.**

#### **References**

**[1]** Schenck JF and Zimmerman EA, NMR Biomed 17(7) 2004. **[2]** Bartha R et al. MRM 47(4) 2002. **[3]** Mitsumori F et al. MRM 62(5) 2009. **[4]** Ye FQ et al. MRM 35 (3) 1996. **[5]** Vymazal J et al. MRM 35(1) 1996. **[6]** Lebel RM and Wilman AH, MRM 64(4) 2010. **[7]** Hallgren B and Sourander P. J Neurochem, 3(1) 1958.

Direct  $R_2$  measurements correlate well with non-heme iron and are very sensitive (iron induced relaxation is equal to spin-spin relaxation at 4.7 T, Fig 3a), but lack specificity due to a confound with the water content/macromolecular fraction [3]. Multiple ESPs reduce the water content confound by measuring changes in the relaxation rate. In this case, the rate of change of  $R_2$  with ESP is linearly depedent on non-heme iron for all regions investigated. The current study excludes the heme iron contribution to brain iron; this may account for some variation observed in Fig 3. The mulitple ESP method is limited by sensitivity and acquisition challenges. Sensitivity increases with field strength, making ultra-high field systems ideal for iron detection with single or multiple ESPs (inherent spin-spin relaxation is largely fieldindependent while iron induced relaxation increases with main magnetic field strength). High field specific acquisition challenges – notably  $B_1$  heterogeneity and SAR  $\vert$ – can be overcome with novel data processing and new acquisition methods. In conclusion, transverse relaxometry at high field is possible. A strong correlation is observed between non-heme iron and  $R_2$ ; multiple ESPs reduce confounds that typically preclude iron measurments with a single ESP and may be a promissing method for iron quantification at high field.

# **Results**

High field quantification of brain iron with<br>
R<sub>2</sub> mapping at multiple interecho spacings<br> **R. Marc Lebel, Catherine A. Lebel, Alan H. Wilman**<br>
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**Figure 1: T2-w images (a, b) and R2 maps (c, d; scaled 0 to 40 s-1). ESP is 6.0 (a, c)**  and 30 (b, d) ms. Contrast and R<sub>2</sub> differences between 6.0 and 30 ms are visible **in the globus pallidus (red arrow) and other basal ganglia structures.**





Interecho Spacing (sec)

**35 year old subject.**

Brain Iron  $(mg/100g)$ 

# **Discussion and Conclusion**

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